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Innovation and Creativity

## **Automatic Blood Glucose Control for Diabetics**

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# Outline

## Introduction

- Diabetes Type I
- Blood Glucose Control
- Previous work

## Automatic Control

- Constraints
- Dynamic Model
- Parameters
- Model Predictive Control

## Conclusion

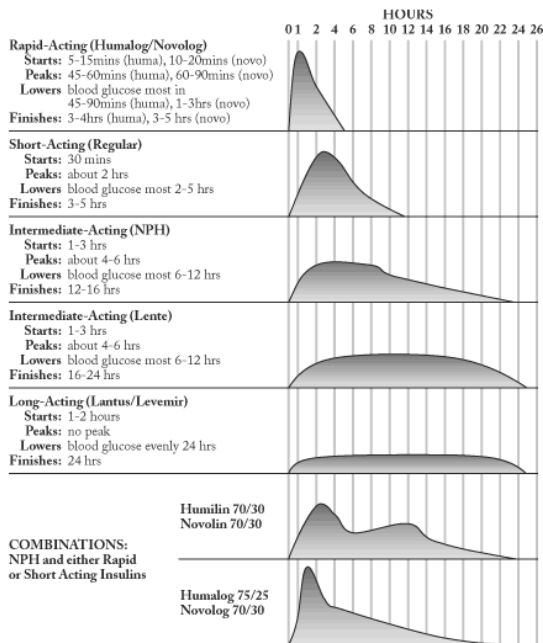
- Future

# Diabetes Type I

- Autoimmune disease
- Deficiency or absence of insulin production
- Autoimmune attack and permanent destruction of the insulin-producing beta cells of pancreas
- Treatment with exogenous insulin via injections
- Hypoglycemia (plasma glucose level  $< 3.5$  mmol/L)
- Hyperglycemia ( $> 7.5$  mmol/L)
- Avoid short- and long-term complications due to hypoglycemia
- Avoid long-term complications due to hyperglycemia
- Control goal: Average plasma glucose  $\approx 5$  mmol/L and never hypoglycemia

# Actuator: Insulin (I)

- Insulin analogs: Effect after 20 minutes, maximum after  $\approx 1$  hour, ends at  $\approx 4 - 5$  hours
- Can be injected continuously, using an insulin pump
- Statement I: We have a slow actuator
- Statement II: Our actuator works only in one direction (down) for the plasma glucose level



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# Insulin Pump



- Insulin compartment (3 mL) lasts for  $\approx 3 - 10$  days
- Soft cannula, must be moved every 3 – 5 days
- Possible to disconnect tube from cannula
- Disconnect for swimming/showering

# Disturbance 1: Food

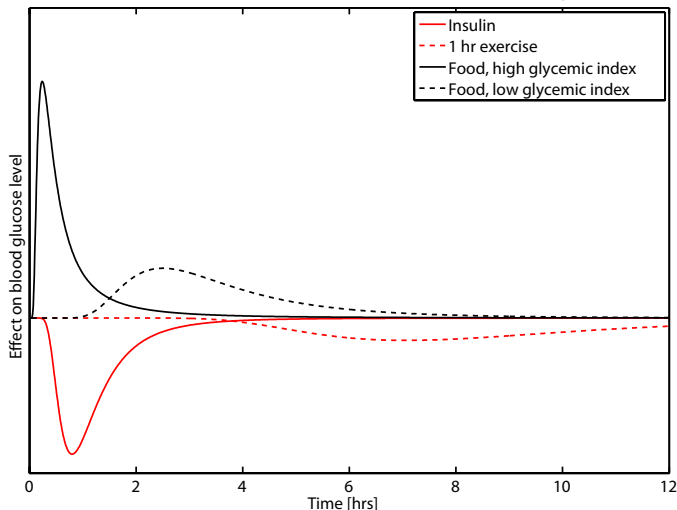
- Effect starts after 10 – 40 minutes, may last for  $\frac{1}{2}$  – 10 hours
- Forward-connection: Possible to predict with measurements in abdomen or in mouth?
- Statement I: This disturbance is often faster than the actuator
- Statement II: This disturbance may vary a lot (depending on the type and amount of food/drink)

## Disturbance 2: Activity

- Effect starts after 30 – 60 minutes, may last for 1 – 72 hours
- Forward-connection: Possible to predict, using a pulse watch
- Statement I: This disturbance is slow, and slower than the actuator



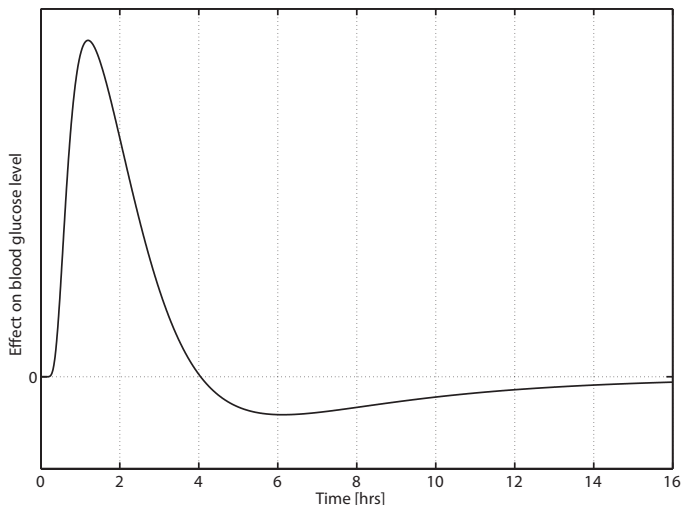
# Actuator and Disturbance Effects



# Special Case: Alcohol

- Effect of the sugar contained in some alcohol drinks (beer): Fast effect (after 10 – 40 minutes), raising the blood sugar
- Effect of alcohol: Slow effect (5 – 10 hours), lowering the blood sugar. Dangerous!

# Alcohol: Effect on Plasma Glucose Level



# Measurements: Plasma Glucose

- Unit: mmol/L in Europe [US: mg/dL]
- Difficult to measure continuously, but it is possible with new technology (although the price is high,  $\approx 200$  NOK/day)
- Not accurate
- Needs calibration (at least two times every day)
- In Norway: Available for testing, from december 2007

# Continuous Glucose Measuring Unit

NOW I CAN chose REAL control around the clock

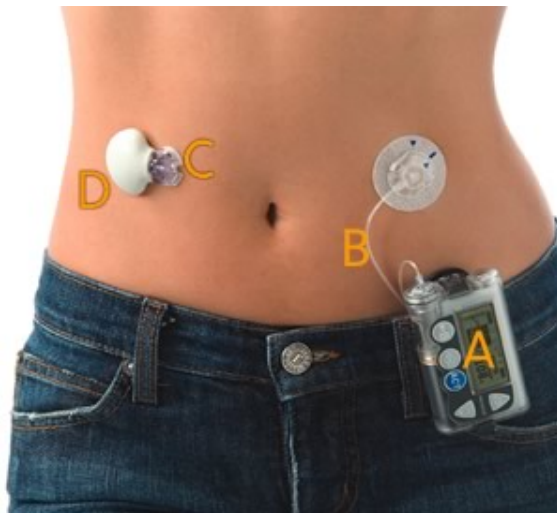


Sensor data is sent continuously to the MiniLink™ Transmitter, which in turn sends data to the MiniMed Paradigm® Insulin Pump through radio frequency (RF) wireless technology.



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# Overall System



- A: Insulin pump
- B: Cannula (soft tube)
- C: Glucose sensor
- D: RF transmitter

# Blood Glucose Sensor: Experiences

- Sensor lifetime  $\approx$  3 days, but sometimes up to 6 days
- Sometimes the sensor does not work at all (gives constant values) and needs to be changed
- Absolute accuracy is quite bad
- Good at showing trends (increasing/decreasing level)
- Alarms (low/high/increasing/decreasing), very useful!
- Simple feedback (turn insulin pump on/off) would be a simple improvement
- Not very user-friendly yet

# 5–6 jan 2008

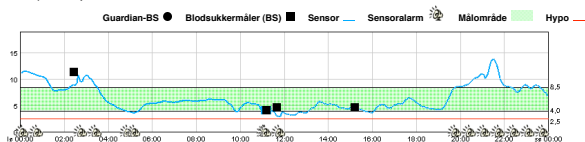


## Daglig sammendrag for Anders Fougner 05.jan.2008

HbA1c: Ingen data

Monitor: Guardian REAL-Time #106871  
Sensor: I bruk

Glukose (mmol/l)

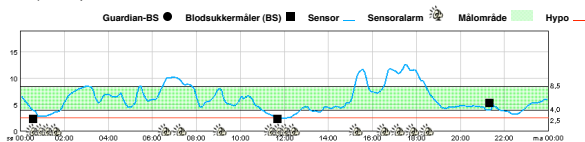


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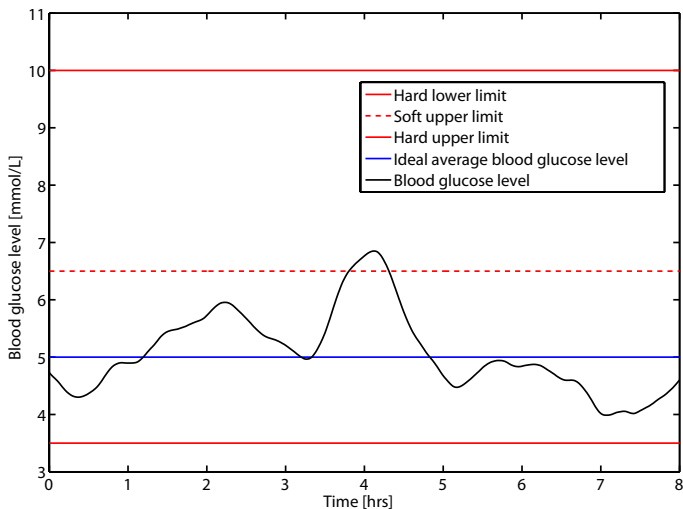




# Previous Work on Automatic Control

- Bergman's (1991) "minimal model" (3 – 5 differential equations)
- The first insulin pumps (1985)
- Fisher (1991) uses the Bergman model for simple open-loop controllers
- Lynch et al. (2002) describes MPC, though based on not-reliable sensors and only simulations
- First reliable sensors (2006)

# Constraints



## Bergman's "Minimal Model"

$$\dot{G} = -p_1 G - X(G + G_B) + D(t) \quad (1)$$

$$\dot{I} = -n(I + I_B) + \frac{u(t)}{V_I} \quad (2)$$

$$\dot{X} = -p_2 X + p_3 I \quad (3)$$

- $G(t)$  - Deviation of plasma glucose concentration [mmol/L] from its basal value  $G_B$
- $I(t)$  - Deviation of free plasma insulin concentration [mU/L] from its basal value  $I_B$
- $X(t)$  - Insulin concentration in the remote compartment

## Bergman's "Minimal Model"

$$\dot{G} = -p_1 G - X(G + G_B) + D(t) \quad (1)$$

$$\dot{I} = -n(I + I_B) + \frac{u(t)}{V_I} \quad (2)$$

$$\dot{X} = -p_2 X + p_3 I \quad (3)$$

- $p_j$  - Parameters describing the dynamics of plasma glucose and insulin interaction
- $D(t)$  - Rate of exogenous infusion of glucose
- $u(t)$  - Rate of exogenous infusion of insulin
- $V_I$  - Insulin distribution volume [L]
- $n$  - Fractional disappearance rate of insulin [/min]

## Bergman's Extended Model (I)

Models a first-order lag of 5 minutes from plasma glucose concentration to subcutaneous glucose.

$$\dot{G}_{sc} = \frac{G - G_{sc}}{5} - R_{ut} \quad (4)$$

- $G(t)$  - Deviation of plasma glucose concentration [mmol/L] from its basal value  $G_B$
- $G_{sc}(t)$  - glucose concentration in subcutaneous/peripherous layer [mmol/L]
- $R_{ut}$  - tissue rate of utilization [mmol/L/min]

## Bergman's Extended Model (II)

Meal glucose disturbance function (very simplified!)

$$\dot{D}_m = -\alpha D_m(t) \quad (5)$$

- $D_m(t)$  - Meal glucose disturbance [mmol/L/min]
- $\alpha$  - Parameter depending on type of food (typically 0.001 – 0.5)

# Parameters (I)

$$V_I = 20 \quad [\text{L}]$$

$$n = \frac{5}{54} \quad [/\text{min}]$$

$$G_B = 4.5 \quad [\text{mmol/L}]$$

$$I_B = 15 \quad [\text{mU/L}]$$

## Parameters (II)

For normal persons:

$$p_1 = 0.028$$

$$p_2 = 0.025$$

$$p_3 = 0.000013$$

For a diabetic:

$$p_1 = 0$$

$$p_2 = 0.025$$

$$p_3 = 0.000013$$



# Model Predictive Control

- Difficulty: The actuator works only in one direction (lowering the plasma glucose level)
- Estimate plasma glucose concentration based on subcutaneous glucose measurements (Kalman filter)
- Performance might be improved with a feed-forward connection (input from the user; food/exercise/etc)
- Simulate before implementing/testing
- Verify the model (now possible)
- Large margins on the first tests

## Constraints (Lynch et al. (2002))

### Input

$$0 \leq u \leq 10 \quad [\text{U/h, where } U = \frac{1}{100} \text{ mL}]$$

### Predicted plasma glucose concentration

$$3.5 \leq \hat{y} \leq 10 \quad [\text{mmol/L}]$$

### Input increments

$$-1.0 \leq \Delta u \leq 1.0 \quad [\text{U/h}]$$

# Future

- Improve the sensors
- Improve and verify the models
- Measure/observe disturbances (feed-forward)?
- Simulate with MPC
- Test MPC on insulin pumps for real diabetics
- Build sensor into cannula
- Lower price for sensors and insulin pumps

# References

- Fisher, M. E. *A Semiclosed-Loop Algorithm for the Control of Blood Glucose Levels in Diabetics*. IEEE Trans. Biomed. Eng., **38**:57–61, 1991.
- Ibbini, M. S., Masadeh, M. A. and Amer, M. M. B. *A Semiclosed-Loop Optimal Control System for Blood Glucose Levels in Diabetics*. J Med. Eng. & Tech., **28**:5:189–196, 2004.
- Lynch, S. M. and Bequette, B. W. *Model Predictive Control of Blood Glucose in Type-I Diabetics Using Subcutaneous Glucose Measurements* Proc. Am. Contr. Conf., pp. 4039–4043, 2002.